

REGULAR ARTICLE

Spectrophotometric nanomolar determination of glucose by using C-dots/Fe₃O₄ magnetic nanozyme

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Abstract. C-dots/Fe₃O₄ magnetic nanocomposite was known as peroxidase-like nanozyme. In this work, C-dots/Fe₃O₄ magnetic nanocomposite was used to determine glucose in the presence of glucose oxidase (GOx). The color change of 3,3',5,5'-tetramethylbenzidine (TMB) was used as an indication of glucose in a colorimetric assay. The nanozymatic activity of C-dots/Fe₃O₄ magnetic nanocomposite to detect glucose was depended on TMB and C-dots/Fe₃O₄ nanozyme concentration and pH. The linear range and detection limit to determine glucose using C-dots/Fe₃O₄ magnetic nanocomposite were obtained as 5×10^{-8} to 1×10^{-3} M and 50 nM, respectively. Also, the sensing system shows high selectivity towards the detection of glucose in the presence of fructose, lactose and maltose as interferences. The results indicate that this assay is simple, cheap, and highly sensitive and selective for glucose determination.

Keywords. Glucose; C-dots/Fe₃O₄ nanocomposite; nanozyme.

1. Introduction

Determination of glucose is one of the most important analytical concerns in biochemistry and biotechnology especially in blood tests and in the production and processing of various kinds of feed and food.¹ Also, the frequent monitoring of glucose is an essential part of diabetes management.^{2,3} In this way, several kinds of electrochemical⁴⁻⁶ and optical^{1,7} methods were implemented for glucose monitoring. But among them, the colorimetric methods are preferred due to its simplification, convenience, continuous monitoring, practically and rapid determinations.^{7,8} Usually colorimetric techniques are employed enzymatic reactions to measure glucose concentration.⁹ In this way, glucose oxidase (GOx) and horseradish peroxidase (HRP) as essential enzymes were implemented extensively in the literature.¹⁰ In a typical cascade reaction as illustrated in Scheme 1, glucose in the presence of GOx enzyme reacts with oxygen to produce gluconic acid and H₂O₂. Then, in the second step, H₂O₂ in the presence of HRP converts a substrate such as TMB (3,3',5,5'-tetramethylbenzidine) to oxTMB which causes the solution to turn blue.¹¹ But natural enzymes have limited applications due to low stability, catalytic dependency on the environmental conditions, high cost and their

difficult recyclability.¹² Therefore, the replacement of nanozyme instead of at least one of the natural enzyme in the above-mentioned colorimetric test for glucose is highly interesting.¹³⁻¹⁷

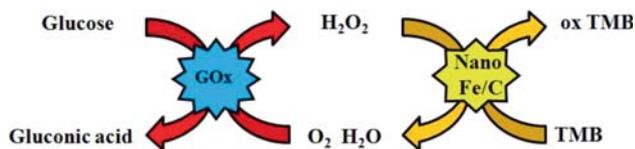
The enzyme-like activity of nanomaterials was investigated recently^{12,18,19} because of the diverse applications of nanozymes/nano enzymes in sensing, imaging, and therapeutics, logic gates, pollutant removal, water treatment, etc.^{20,21} Consequently, carbon,^{8,11,14,22,23} noble metal^{15,16,24,25} and metal oxide-based²⁶⁻³² nanomaterials prove to be the promising ones. In this way, the C-dots/Fe₃O₄ magnetic nanocomposite was synthesized previously.^{33,34} This nanocomposite showed intrinsic peroxidase-like activity and was used to determine H₂O₂.³³ In the present work, the ability of C-dots/Fe₃O₄ magnetic nanocomposite as peroxidase-like nanozyme was used for colorimetric determination of glucose.

2. Experimental

2.1 Materials and synthesis

Carbon soot was obtained by burning a candle. Glucose was purchased from Merck. All other chemicals with analytical grade were obtained from Sigma-Aldrich. C-dots/Fe₃O₄ magnetic nanocomposite was prepared by using the previously reported procedure.³³ Briefly, carbon soot (25 mg)

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Schematic 1. Schematic illustration of colorimetric detection of glucose using GOx and HRP.

was refluxed in nitric acid (5M) and after centrifugation, the light brownish-yellow supernatant was used as C-dots. Also, magnetic iron oxide nanoparticles were prepared in alkali media based on the previously reported procedure.³⁵ Briefly, ammonia was rapidly injected to the solution of Na_2SO_3 (0.16 mol L^{-1}) and FeCl_3 (0.05 mol L^{-1}) and heated at 60°C for 30 min. After 2 h, the magnetic Fe_3O_4 powder was isolated by using a permanent magnet (1.4 T). Then solutions of Fe_3O_4 nanoparticles and C-dots were mixed together by the ratio of 1:4 in pH2 to prepare nanocomposite. And after 30 min, the as-prepared nanocomposite was separated by a permanent magnet. Finally, the obtained nanocomposite was washed two times with distilled water.

2.2 Instrumentations

The morphology of the samples was determined by using a Zeiss, EM10C electron transmission microscope (80 kV).

TESCAN VEGA3 was used as energy dispersive spectroscopy (EDS). A D8 ADVANCE type (BRUKER-Germany) X-ray diffractometer (XRD) with $\text{Cu-K } \alpha$ radiation was used to identify the structure ($\lambda = 0.1542 \text{ nm}$). UV-Vis spectra were collected by using Hach DR 5000 spectrophotometer. Also, the pH measurements were performed using a Metrohm pH meter (model 780).

2.3 Procedure for colorimetric determination of glucose

For glucose detection, at first solutions of different concentration of glucose and $50 \mu\text{L GOx } 100 \text{ U mL}^{-1}$ were incubated for 30 min. Then 1 mg nanocomposite, 2.1 mL acetate buffer pH 2.4 and $500 \mu\text{L TMB } 1.2 \text{ mg mL}^{-1}$ were added into the solutions. Then visible spectra were collected after 15 min.

3. Results and Discussion

3.1 Structural characterization

Structural analysis of C-dots/ Fe_3O_4 magnetic nanocomposite was performed by using TEM, EDS and XRD (Figure 1). TEM image depicts the presence of both C-dots and Fe_3O_4 nanoparticles with different sizes in

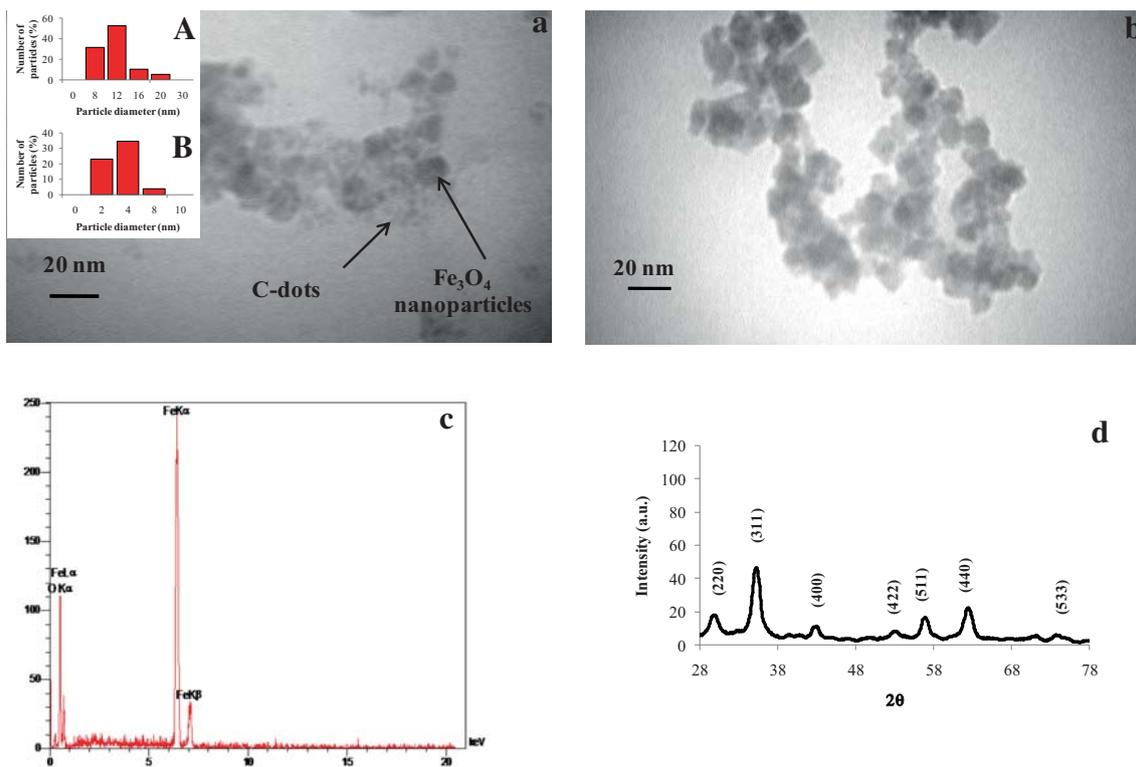


Figure 1. TEM images of (a) C-dots/ Fe_3O_4 and (b) Fe_3O_4 nanocomposite (Inset: particle size distribution of (A) Fe_3O_4 NPs and (B) C-dots), (c) EDS pattern and (d) XRD pattern of C-dots/ Fe_3O_4 magnetic nanocomposite.

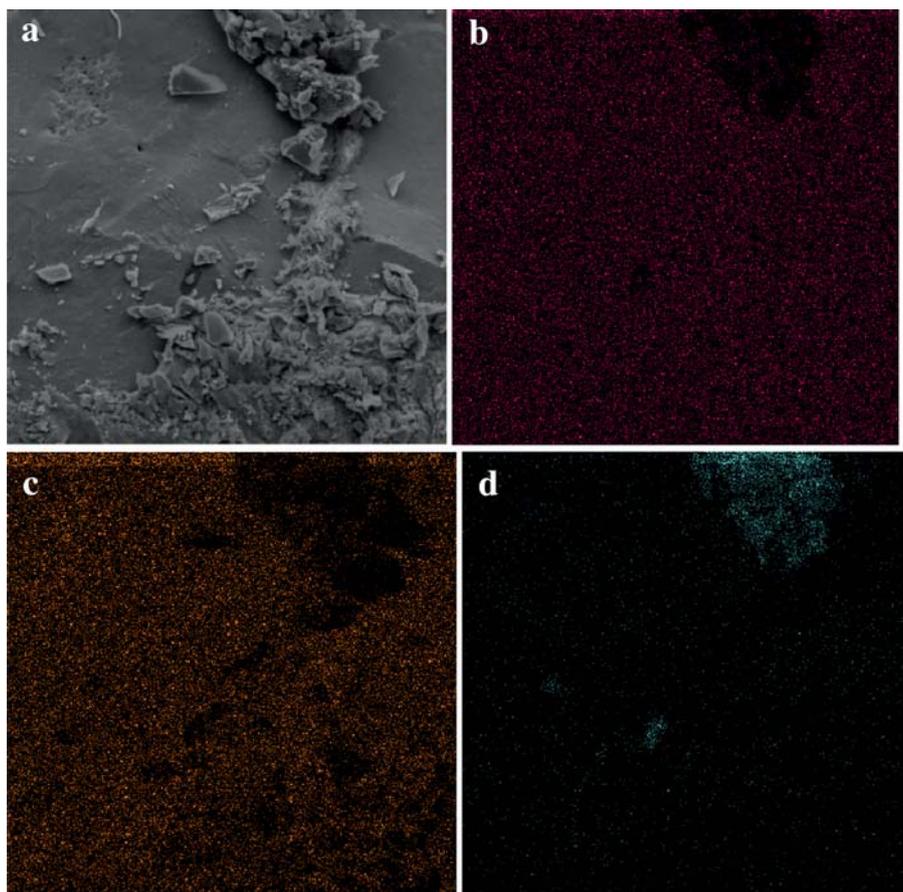


Figure 2. (a) Scanning electron microscopy and elemental mapping of (b) Fe, (c) O and (d) C.

the as-prepared nanocomposite structure (Figure 1a). Clearly, C-dots (average diameter ~ 4 nm) are smaller than Fe_3O_4 nanoparticles (~ 12 nm). For better comparison, the TEM image of Fe_3O_4 nanoparticles presents in Figure 1b. Also, X-ray energy dispersive spectroscopy (EDS) analysis shows the presence of carbon, iron and oxygen elements in the nanocomposite (Figure 1c). Elemental mapping of the nanocomposite presents in Figure 2. Clearly, iron and oxygen are homogeneously distributed while carbon is localized in specific areas within the precipitate. At XRD pattern of nanocomposite (Figure 1d), corresponding peaks of Fe_3O_4 nanostructures at 30.1° , 35.7° , 43.1° , 53.5° , 56.9° , 62.6° and 74.2° can be observed which are related to the Miller indices of (220), (311), (400), (422), (511), (440), and (533), respectively. So, the spinel structure of Fe_3O_4 nanoparticles was confirmed by observed indices.³⁶ So, the XRD pattern of nanocomposite depicts the presence of iron oxide as Fe_3O_4 in the nanostructure. As a result, Fe_3O_4 nanoparticles preserve their structure in the nanocomposite. So, the C-dots/ Fe_3O_4 magnetic nanocomposite was synthesized properly based on the previous report.³³

3.2 Determination of glucose using GOx and C-dots/ Fe_3O_4 magnetic nanocomposite

The peroxidase-like activity of C-dots/ Fe_3O_4 magnetic nanocomposite has been explored previously.³³ By using this nanozyme, nano-molar determination of hydrogen peroxide was possible. The main advantage of the C-dots/ Fe_3O_4 magnetic nanocomposite is its higher peroxidase-like activity rather than individual Fe_3O_4 magnetic nanoparticles and C-dots.³³ So, in this study, the presence of C-dots/ Fe_3O_4 magnetic nanocomposite instead of HRP for determination of glucose was tested. In this way, the effect of the presence of C-dots/ Fe_3O_4 magnetic nanozyme and GOx in successive reactions for the determination of glucose was examined. Since GOx would be denatured in acidic pH solution, the glucose detection using peroxidase-like nanozymes and GOx usually were performed in two steps with two different pH values.¹¹ In fact, at first, glucose reacts with oxygen in the presence of GOx in the mild conditions, i.e., $\text{pH} = 7.0$ and then the produced hydrogen peroxide in other pH condition were detected in the presence of peroxidase-like nanozymes. In the presence

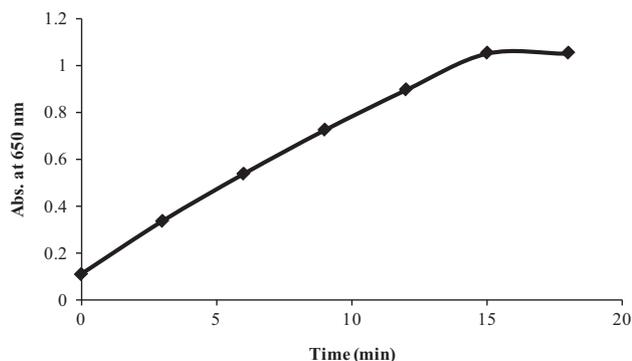


Figure 3. Dependency of absorption at 650 nm on time for glucose detection in the system contains C-dots/Fe₃O₄ magnetic nanocomposite.

of peroxidase-like active nanozyme the solution color change to blue due to the presence of TMB. In this manner, by addition of a solution of glucose and GOx to the solution containing C-dots/Fe₃O₄ magnetic nanocomposite and peroxidase substrate, i.e., TMB, a blue color reaction was produced, indicating that C-dots/Fe₃O₄ magnetic nanocomposite has peroxidase-like catalytic activity (Figure 3). The controlled experiments with C-dots/Fe₃O₄ in the absence of GOx and vice versa do

not show any significant peak at 650 nm. The catalytic reaction was monitored by TMB absorbance change at 650 nm. The time-dependent absorbance changes of TMB are depicted in Figure 3. Clearly, an increase in absorption at 650 nm was observed by increasing the time. After 15 min, the plot reaches the plateau and enzymatic activity reaches a maximum value.

Furthermore, the dependency of C-dots/Fe₃O₄ magnetic nanocomposite activity on TMB and nanozyme concentration and also pH was investigated (Figure 4). The nanozymatic activity of C-dots/Fe₃O₄ magnetic nanocomposite such as natural enzyme depends on the concentration of substrate concentration, i.e., TMB, nanozyme concentration and pH. Also, the maximum relative activity of C-dots/Fe₃O₄ magnetic nanocomposite was observed at $\sim 0.4 \text{ mg mL}^{-1}$ TMB and $400 \mu\text{g mL}^{-1}$ nanocomposite. However, it was found that the C-dots/Fe₃O₄ magnetic nanocomposite exhibited a strong peroxidase-like catalytic activity at a strongly acidic medium, i.e., pH = 2.0 (Figure 4). These observations are well demonstrated that the C-dots/Fe₃O₄ magnetic nanocomposite possess a high degree of activity and stability as peroxidase catalysts in the harsh condition of pH = 2.0.

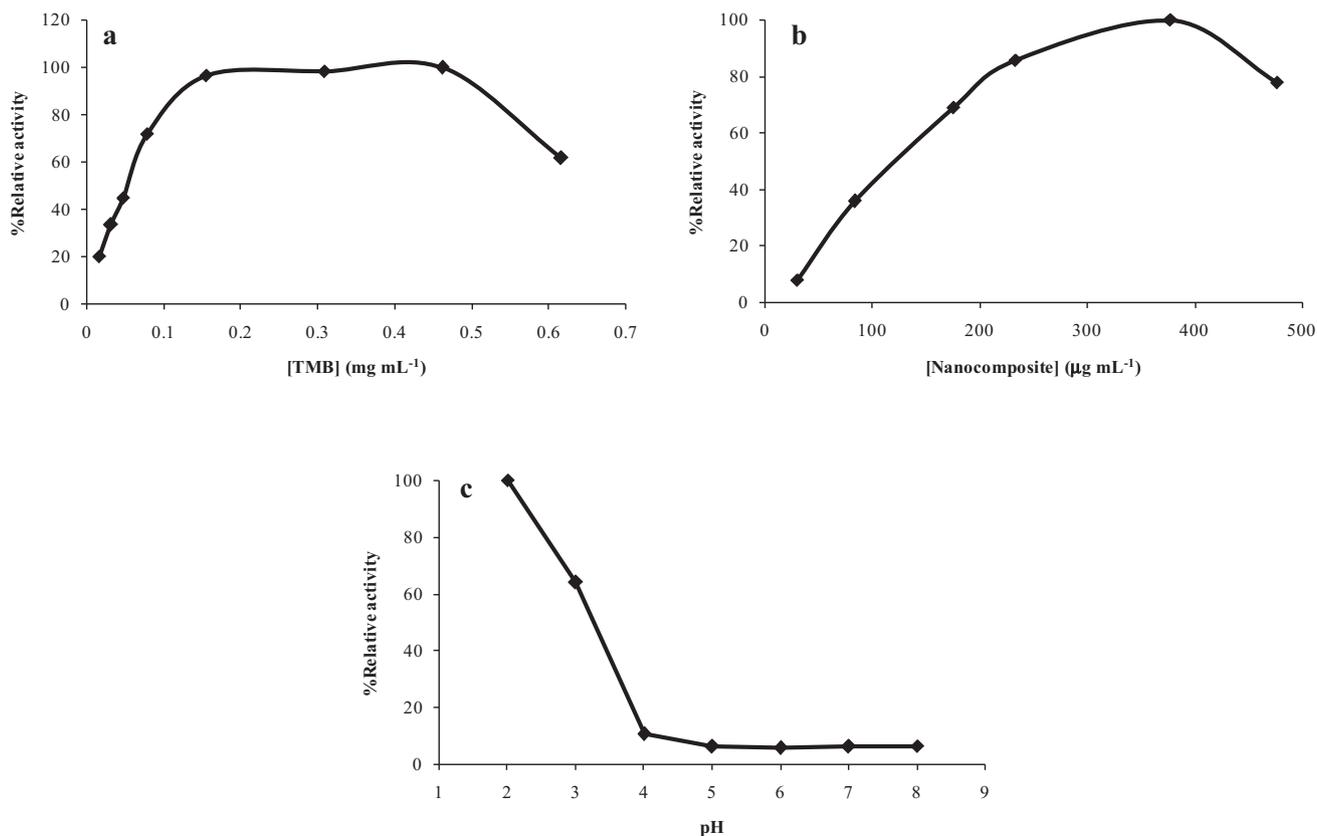


Figure 4. Dependency of absorption spectra on (a) TMB concentration, (b) C-dots/Fe₃O₄ magnetic nanocomposite concentration and (c) pH in presence of GOx and C-dots/Fe₃O₄ magnetic nanocomposite.

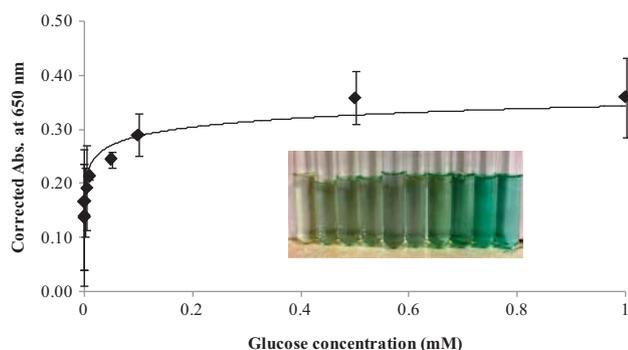


Figure 5. Calibration plots for glucose detection using GOx and C-dots/Fe₃O₄ magnetic nanocomposite (inset: corresponding photograph).

On the basis of the above results, C-dots/Fe₃O₄ magnetic nanocomposite was implemented for the determination of glucose. A calibration curve was attained (Figure 5), which demonstrated a logarithmic relationship between the absorbance and the glucose concentration ranging from 5×10^{-8} to 1×10^{-3} M. The equation of the corresponding curve is $Corrected\ Abs. = 0.024 \ln([glucose](mM)) + 0.344$ with $R^2 = 0.927$. The detection limit (DL) for glucose was obtained experimentally as 5×10^{-8} M. Table 1 summarizes the figures of merit for determination of glucose and compares the results with previously reported nanozymes. Clearly, in this case, the determination range was expanded to three orders of magnitude larger, and detection limit was also improved one or three order of magnitude rather than C-dots and Fe₃O₄ magnetic nanoparticles, respectively.

To investigate the selectivity of the proposed method the response of fructose, lactose, and maltose as glucose analogues were recorded. The results (Figure 6) demonstrated that the absorbance of these interferences was negligible compared to that of glucose even at concentrations as high as 5 mM. Therefore, this biosensing system indicates high selectivity for glucose due to the high affinity of glucose oxidase for glucose.

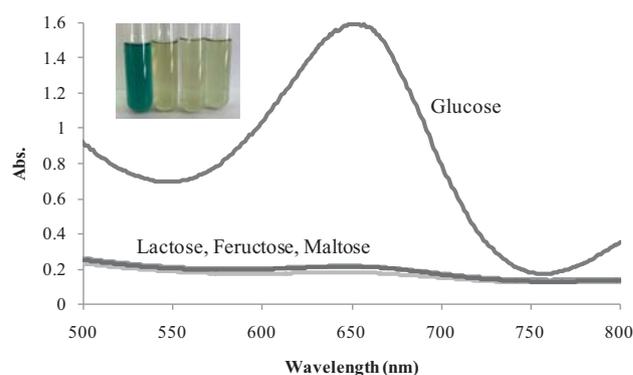


Figure 6. Spectra of 5mM glucose, fructose, maltose and lactose using GOx and C-dots/Fe₃O₄ magnetic nanocomposite (inset: corresponding photograph).

Also, the reproducibility of the proposed method was examined. RSD of 10.2% was obtained for three times determination of $1 \mu\text{M}$ glucose which is an acceptable value for precision. Moreover, the determination of glucose in human serum was performed to test the wider utility of the nanocomposite. The exact amount of glucose in the real sample was 100 mg dL^{-1} , while the obtained value using the proposed procedure was 109.5 mg dL^{-1} . In this way, a relative deviation of 9.5% was obtained for the determination of glucose.

4. Conclusions

Performance of C-dots/Fe₃O₄ magnetic nanocomposite in the presence of GOx for determination of glucose was investigated. The response of the proposed assay was dependent on pH, TMB and nanocomposite concentrations. Figures of merit for introduced assay were calculated. The obtained linear range was wider than other previous similar reports. Also, the proposed methodology to determine glucose is simple and cheap and most importantly, determination in nanomolar level is possible.

Table 1. Figures of merit for colorimetric determination of glucose by the use of various peroxidase-like nanozymes and GOx in cascade reactions.

Implemented nanozyme	Determination range (M)	DL (M)	References
Fe ₃ O ₄ nanoparticle	$5 \times 10^{-5} - 1 \times 10^{-3}$	3×10^{-5}	37
C-dots	$1 \times 10^{-6} - 5 \times 10^{-4}$	4×10^{-7}	38
Graphene oxide-Fe ₃ O ₄ nanocomposites	$2 \times 10^{-6} - 2 \times 10^{-4}$	7.4×10^{-7}	28
Casein-Fe ₃ O ₄ nanocomposite	$3 \times 10^{-6} - 1 \times 10^{-3}$	1×10^{-6}	39
C-dots-Fe ₃ O ₄ nanocomposite	$5 \times 10^{-8} - 1 \times 10^{-3}$	5×10^{-8}	This work

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